An evaluation of the effect of different veneer materials on fracture resistance of zirconia core

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ABSTRACT

Objectives: this in vitro study was done to evaluate the effect of packable P60 composite and Tetric N-Ceram composite veneer material on fracture strength of zirconia cores. Material and Methods: Twenty four zirconium cores (Vita, Germany) with 0.7 mm thickness were fabricated by CAD/CAM technology and then subjected to air abrasion with 50 µm of Al₂O₃. Cores were randomly divided into three groups according to veneering material (group A: control group sandblasted with 50 µm Al₂O₃ veneered by IPS E-max Ceram porcelain, group C: sandblasted with 50 µm Al₂O₃, etching with hydrofluoric acid and veneered with P60 composite, group E: sandblasted with 50 µm Al₂O₃, etching with hydrofluoric acid and veneered with Tetric N-Ceram composite). All crowns were subjected to fracture strength test in the testing machine, with load application by steel ball indenter and 0.5 mm/min. cross head speed. Results: statistical analysis was carried out utilizing one-way ANOVA, LSD. The results of fracture strength value test showed the highest mean value was registered for group (A), and the lowest mean for group (E). One-way ANOVA test represented that, there was a statistically high significant different among all groups. LSD results showed a high significant difference increase in fracture resistance for Group A at p value (*p < 0.001 High
**INTRODUCTION**

Ceramics are broadly utilized as materials for restorations because of the ideal characteristics like biocompatibility esthetics and strength. One of the most utilized ceramic in dentistry is Yttria partially stabilized zirconia (Y-TZP) for fabricating frameworks because of its superior optical and mechanical characteristics [1]. All-ceramic crowns or crowns double layer composed of a highly strength ceramic framework such as alumina or zirconia that veneered with dental porcelain for example feldspathic porcelain. In spite of the consequent restorations have ideal esthetic characteristics, but these restorations subject to failure like fracture of the veneering porcelain [2].

Veneering ceramic can’t resisted high tensile stress that finally cause fracture in ceramic. Ceramic restorations likewise may cause wear and abrasive to the opposing teeth [3,4]. Recently, veneering zirconia substructure with high strength indirect composite resin has been proposed as an alternative veneering method to the conventional porcelain veneering system [5].

Composite resins materials are broadly utilized for direct restorations because of their ideal mechanical, optical and physical characteristics, simplicity of manipulating also capacity to be bonded with the tooth structure. [6] To veneer zirconia with composite resins, the bonding between the composite resin and zirconia is a crucial factor. Superior bond strength between the veneering composite resin and zirconia substructure was found in an vitro study by using a zirconia primer [7].

The objective of this study was to investigate the fracture load to failure of the composite veneered zirconia crowns preparing with two different zirconia surface treatments.

**MATERIAL AND METHODS**

A master metal die was constructed from an ideal pre-prepared plastic right maxillary first molar (Nissin Dental Products, Kyoto Japan), having deep chamfer finishing line (0.8 mm), (2 mm) reduction occlusally. The metal die was fabricated by using “CAD / CAM system” in order to simulate the shape of an ideal prepared plastic die, so that the all ceramic crowns were received [8].

The plastic die was sprayed with dental scan spray, so the reflection of light during scanning process was inhibited. The distance between the plastic die and the nozzle of scan spray bottle was (7 cm) depending to the manufacturer’s guidelines. The distance was calculated by placing the die on bech, measuring 7cm with a ruler from the tip pf spray. The plastic die was inside the dental scanner unit (DOF, full HD, 5M pixel; Korea) w and fixation on scan stage by special clay was done.

A three dimensional image was taken so
that all surfaces and finishing line of plastic die were appeared clearly [9]. The digital model of the die transferred to the CAM software to start the dry milling process of the metal die by using the milling unit which was loaded with cobalt chromium disc (10 mm) (Interdent, Travagliato(BS) Italy).

**Base construction of metal die**

The base for the metal die was constructed from dental stone type IV to allow proper position of the metal die during scanning. Two grooves were made in the bottom of the metal die for retention of the stone base to the metal die. The dental stone was blended depending to manufacturer guidelines the dental stone was blended (100 g powder/ 20 ml water), vibrated, and poured to 4 mm below the cemento-enamel junction [10] (Figure 1). The stone base was separated from the plastic ring after 40 min according to the manufacturer’s instructions. The metal die was surface scanned in the same way as in scanning of plastic die.

**Milling of zirconium core**

The suitable Yttria-stabilized zirconia blank was positioned inside the milling apparatus in the blank holder and it was secure with the screw driver, at that point milling procedure was begin. When milling procedure was ended, the zirconia disc was taken away from the holder and the cores framework were disconnected from the disk via disk bur with a laboratory hand piece. The cores were positioned inside sintering furnace and the sintering was performed depending to the manufacturer’s recommendations.

**Sandblasting the Zirconium Cores**

Following sintering, the surface of the zirconium cores were subjected to an air abrasion procedure with (50µm) Al$_2$O$_3$ particles at pressure (1.5) bar for (10) sec, and sandblasting procedure was at (10) mm fixed distance between the nozzle and the core surface.

The nozzle can be moved in up-down movement without affecting the constant distance between the nozzle and specimen, so all parts of the working surface of core were exposed to sandblast particles during sandblasting procedure, following sandblasting, cleaning with steam jet cleaner was performed for all specimens.

**Sample grouping**

Twenty four Zirconia were divided to three groups according to the veneering materials used: (The specimens’ numbers was based on previuos studies).

- **Group A:** 8 cores were sandblasted and veneered with IPS e.max ceram porcelain (control group).
- **Group C:** 8 cores were sandblasted and used Glaze-on technique by surface treated with Hydrofluoric acid (9.5%) and bonding agent added, then veneered with 3M ESPE Filtek Packable P60 Composite resin.
**Group E:** 8 cores were sandblasted and used Glaze-on technique and surface treated with Hydrofluoric acid (9.5%) and bonding agent added, then veneered with Tetric Ceram Composite resin.

In group (A), a silicon index was fabricated from putty condensation silicon impression material (Zhermack, Italy) so, an impression was taken to celluloid crown over zirconia core in order to control the thickness of veneering material (2 mm) The index from silicon was made according to manufacturer recommendations by mix up the base with catalyst of the putty condensation silicon rolled into a ball and placed onto a composite crown, then pressed until setting. After complete set, the index was taken away and divided longitudinally from bucco-palatal direction via a surgical blade No.12 [12].

In order to apply veneering ceramic on zircon, the layering technique was used by mixing ceramic powder (50 mg) of IPS E.max Ceram, dentin A3. (Ivoclar Vivadent, Schaan, Liechtenstein, Germany). The powder was mixed with (3 drops) of their special liquid to produce the desired creamy consistency of ceramic (wash dentin) it was applied to the prepared core surface by a brush, with light vibration , excess liquid was blotted with paper tissue, then firing process of ceramic/dentin was performed in the ceramic furnace according to the manufacturer instructions. In the same manner, The 2nd layer of dentin and enamel porcelain layer were applied in the same manner over the 1st layer and vibrated, it was dried and fired according to the manufacturer instructions. When firing was completed, the dimensions of veneering ceramic were checked by index and Vernier. Sintering furnace cycle for ceramic veneer was illustrated in Table I.

For group (C), the surface of zirconium cores was coated with a very thin layer of glazing porcelain and sintered with glaze firing protocol according to manufacturer's instructions. This procedure called (glaze-on) technique [13].

The glazed surface of zirconia core was etched with hydrofluoric acid (9.5%) for 30 sec, then rinsed with water spray for 60 sec to remove all acid residual and dried with oil-free compressed air.

Prior to composite resin application, Single Bond Universal Adhesive (3M ESPE, USA) was applied on the etched surface and rubbed using disposable brush and lightly air dried for 2 sec, then the bond was subjected to light cure for (20 sec).

A disposable celluloid crown was used to obtain the desired and uniform composite veneering thickness to all composites groups, it was used as a mold for composite resin after adjusted its edge with the die margin and the excess was removed with small scissor. Packable Filtek P60 composite resin was adapted into the celluloid crown. A light cure unit with a power intensity of 600 mw / cm² for 20 sec was used for curing the occlusal, buccal, palatal, mesial and distal surface according to manufacturer's recommendations. After the curing procedure was completed, celluloid crown was removed from the restoration.

For group (E): The same procedure of glaze-on technique (etching, bonding, and application of composite resin veneering material) was done as the same manner in group (C) and Tetric N-Ceram composite resin was used as the veneering material. The composition and manufacturers for composite resins used was illustrated in Table II.

For testing fracture resistance, each crown was seated on metal die but without cementation. All crowns were subjected to load to failure test in a universal testing machine (Lloyd LRX-Plus, Lloyd instruments Ltd. Fareham Hants, UK) with a steel ball indenter with a (6 mm) diameter, the cross head speed of (0.5 mm./min) the load was applied occlusally in the (fossa) then, registered in Newton the extreme load causing crown fracture [13] (Figure 2).
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The procedures and mechanical test were performed by both authors.

![Image](making-stone-base-to-metal-die.png)

**Failure mode**

Failure modes of the fractured specimens were investigated using visual inspection. Two failure modes were categorized as follows: (a) chipping of veneering materials and (b) fracture of core materials and veneering materials together or total fracture.

**RESULTS**

The descriptive statistics of the values of fracture resistance including: the means, standard deviation, with minimum and maximum values for each veneered groups as shown in table III.

**Table III** - Descriptive Statistics of fracture resistance of veneered groups (A, C, E) in (Newton)

<table>
<thead>
<tr>
<th>Group</th>
<th>Minimum</th>
<th>Maximum</th>
<th>Mean</th>
<th>Std.Error</th>
<th>SD</th>
</tr>
</thead>
<tbody>
<tr>
<td>A</td>
<td>1721.65</td>
<td>1978.92</td>
<td>1826.4575</td>
<td>38.59839</td>
<td>109.17273</td>
</tr>
<tr>
<td>C</td>
<td>1331.95</td>
<td>1716.75</td>
<td>1582.4713</td>
<td>41.56172</td>
<td>117.55428</td>
</tr>
<tr>
<td>E</td>
<td>1092.40</td>
<td>1275.30</td>
<td>1217.0156</td>
<td>24.22378</td>
<td>68.51520</td>
</tr>
</tbody>
</table>

Table III demonstrated, the highest mean of fracture resistance values were in group (A), while the lowest mean of fracture resistance values were for group (E).

One-way analysis of variance (ANOVA) test was done to assess whether there is statically significant difference or not in the mean value among the three groups of veneering zirconium cores, as shown in table IV.

**Table II** - Composition and manufacture of composite resin used in this study

<table>
<thead>
<tr>
<th>Product</th>
<th>Filtec P60</th>
<th>Tetric N-Ceram</th>
</tr>
</thead>
<tbody>
<tr>
<td>Manufacture</td>
<td>3M Dental Products (USA)</td>
<td>Ivoclar Vivadent (Schaan/Liechtenstein)</td>
</tr>
<tr>
<td>Composite Type</td>
<td>Packable</td>
<td>Nano-Hybrid Composite</td>
</tr>
<tr>
<td>Method of Activation</td>
<td>Visible Light cure</td>
<td>Visible Light Curing</td>
</tr>
<tr>
<td>Resin Components</td>
<td>Bis-GMA, UDMA, Bis-EMA.</td>
<td>Bis-GMA, UDMA, Dimethacrylates (Bis-GMA, UDMA)</td>
</tr>
<tr>
<td>Filler Type</td>
<td>Zirconia/Silica</td>
<td>Barium Glass, Ytterbium Trifluoride, Mixed Oxide and Copolymers</td>
</tr>
<tr>
<td>Filler Particle Size Range</td>
<td>(0.01-3.5) µm</td>
<td>(40-3000) nm</td>
</tr>
<tr>
<td>Filler Loading (Wt./Vol.)</td>
<td>83%wt. / 61% vol.</td>
<td>80-81% wt. 55-57% vol.</td>
</tr>
<tr>
<td>Curing Time</td>
<td>20 sec</td>
<td>20 sec</td>
</tr>
</tbody>
</table>
DISCUSSION

In order to control several of the disadvantages related with veneering porcelain with zirconia crown, zirconium substructure veneered with composite was suggested. Such crowns are fabricated with a light cure composites, the advantages of this method incorporate strength, minimal abrasive, biocompatibility of zirconia framework, composite veneer permits simplicity of application also repair intra orally [14-19].

In the present study, the load- to- failure tests or occlusal fracture strength is the one process to examine the structural solidity of that structures which takes into consideration the various component layers and the complications of the crowns anatomy [20]. The cross head speed of 0.5 mm/min. load was applied to the center of the crown by 6mm diameter stainless steel ball [13].

The results of the present study showed a high fracture resistance value in group A and the lowest fracture strength value was in group E this could be explained by that the sandblasting not only brings about morphological changes of material surface, but also increases adhesion efficiency. Also, one prospective factor is the lack of primary stability of zirconia by its transformation from the tetragonal into monoclinic crystallographic phase as an effect of the presence of moisture and elevated temperature [21].

The results of the present study comes in agreement with Su et al. [22] a study showed that sandblasting procedure is a significant surface management that could enhance the bond strength between veneering material and zirconia, and this fine powder particles was more abrasive safely more zirconia was taken off via 50 um of powder particles.

HF was used as a method of treatment have been recommended to improve the bonding strength between zirconia and veneering porcelain by creating micromechanical interlocking [23].
The result of the present study showed a high significant difference for both group C and group E when compared with group A. This could be explained that “Hydrofluoric acid” is utilized when the matrix composed of silicates or silica. Initially, silicon tetrafluoride was formed. Tetrafluoride fuse with hydrofluoric acid to form soluble complex ion(hexafluorosilicate) which in turn reacts with hydrogen protons to form tetrafluorosilicic acid, a product that can be selectively removed by water, and the crystalline structure is un covered the outcome surface of the ceramic become rough [24].

The results of this study comes in agreement with Guazzato et al., [14] a study showed that in the adherance of all ceramic restorations, alteration in the surface morphology, just like pores and grooves, are considered important. Both chemical bonding and micro-mechanical interlocking to the surface of ceramic raise the fracture strength of the restoration and the restored tooth, prevent microleakage, improve marginal adaptation and provide high retention.

The result of the current study revealed significant result when comparing all the groups. This could be explained, in packable P60 Filtek, manufactures have increased the filler contact and reduce the average filler particle size by using excessive proportion of irregular (blend of different size glass rods, or particles) or porous filler. In general, packable are loaded in excess of 80% by volum, [25] while the “Tetric Evo Ceram” are generally loaded of 60% by volum, [26] to raising the viscosity, reduce the quantity of resin and creating the particular manipulation property [27]. Packable contain less resin matrix (29% volume) in addition, types of fillers are zirconium and “silica” fiber in which silica scatter light [25].

Moreover, the elevation in the fracture strength of restored teeth might be referred to that composite material utilized in the present study are count less-shrink material, also it had been demonstrated that the utilize of less-shrinkage composites material enhanced the fracture strength of restoration. This results comes in a concurrence with [28] a study deduced that the utilize of less shrink composite material safely reinforced under compression loadings.

As a conclusion, within the limitation of this study, using conventional sandblasting with 50 µm Al₂O₃ and veneering with conventional ceramic produced restoration with acceptable fracture resistance value.

Clinical significance: veneerizing zirconia core with direct resin composite restoration considered as an alternative method for replacement of chipped or fractured ceramic veneer.

REFERENCES
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Braz Dent Sci 2021 Jul/Sep;24(3)

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Date submitted: 2020 Jul 16
Accept submission: 2020 Oct 19


25. 3M ESPE technical product profile filtekTM P60 Universal Restoration. 3M ESPE [Internet]. St. Paul, MN, USA; 2016. Available from: https://multimedia.3m.com/mws/media/4449003-3m-filtek-p60-posterior-restorative-technical-product-profilepdf

